

Having thus described the preferred embodiments, the invention is now claimed to be:

1. A method for calibrating a coincidence imaging system which includes a plurality of radiation detectors, 5 the method comprising:

measuring a plurality of coincidence radiation events associated with a point radiation source;

assigning initial values for a set of fitting parameters;

10 applying a minimization algorithm including:

calculating lines of response (LOR) based upon the fitting parameters and the measured radiation events,

generating a figure of merit characterizing 15 the apparent size of the point radiation source based upon the LOR's, and

optimizing the fitting parameters to produce a minimized figure of merit;

20 and

extracting from the optimized fitting parameters a correction factor relating to a positional coordinate of a detector.

2. A method for imaging using a plurality of 25 radiation detectors, the method comprising:

measuring a plurality of coincidence radiation events associated with a point radiation source;

assigning initial values for at least one fitting parameter;

30 calculating lines of response (LOR) based upon the at least one fitting parameter and the measured radiation events;

generating a figure of merit characterizing the apparent size of the point radiation source 35 based upon the LOR's;

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optimizing the at least one fitting parameter using
a minimization algorithm which includes
iteratively repeating the calculating and
generating steps to produce a minimized figure
of merit;

5 extracting from the at least one optimized fitting
parameter at least one correction factor;

acquiring a set of radiation data from an associated
subject;

10 correcting the radiation data for camera misalignment
by correcting the spatial coordinates of the
detected radiation events using the at least one
correction factor; and

15 reconstructing an image representation from the
corrected radiation data.

3. The imaging method as described in claim 2,
wherein the at least one fitting parameter includes:
a parameter related to the radial positional
coordinate of a detector.

20 4. The imaging method as described in claim 2,
wherein the at least one fitting parameter includes:
a parameter related to the tangential positional
coordinate of a detector.

5. The imaging method as described in claim 2,
25 wherein the at least one fitting parameter includes:
a parameter related to the orientational positional
coordinate of a detector.

6. The imaging method as described in claim 2,
wherein:
30 the step of generating a figure of merit includes
summing a distance of closest approach of each
LOR to a spatial point; and

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the at least one fitting parameter includes the positional coordinates of the spatial point.

7. The imaging method as described in claim 2, wherein:

5 the step of generating a figure of merit includes summing the square of a distance of closest approach of each LOR to a spatial point; and the at least one fitting parameter includes the positional coordinates of the spatial point.

10 8. The imaging method as described in claim 7, wherein the step of generating a figure of merit further includes:

discarding LOR's whose distance of closest approach is greater than a preselected distance.

15 9. The imaging method as described in claim 2, wherein the step of generating a figure of merit further includes:

obtaining a crossing point of each pair of LOR's; and calculating a standard deviation of the crossing 20 points.

10. The imaging method as described in claim 2, wherein the step of generating a figure of merit further includes:

25 obtaining a distance of closest approach for each pair of LOR's; and calculating a standard deviation of the obtained distances.

11. The imaging method as described in claim 2, wherein the number of detectors is N and the fitting 30 parameters include:

Δr_i , $i=1$ to N , where Δr_i is a correction for the radial coordinate of the i th detector;

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Δt_j , $j=1$ to N , where Δt_j is a correction for the tangential coordinate of the j th detector; and $\Delta \theta_k$, $k=2$ to N , where $\Delta \theta_k$ is a correction for the orientational coordinate of the k th detector.

5 12. The imaging method as described in claim 11, wherein the fitting parameters further include:
 positional coordinates of the point radiation source.

10 13. A method of PET imaging comprising:
 coincidence detecting radiation events from a calibration source with at least two detector heads;
 calculating correction factors that correct for mechanical misalignment of the detector heads from the coincidence detected calibration source radiation;
15 during a diagnostic imaging procedure performed on a subject, generating image data in response to radiation collected with the detector heads;
 correcting the image data with the correction factors; and
20 reconstructing the corrected image data into an image representation.

25 14. A coincidence imaging system comprising:
 a gantry;
 a plurality of flat panel detectors disposed about the gantry;
 a data memory which stores measured data about radiation events detected by the detectors;
 a calibration memory which stores a plurality of calibration parameters for correcting data measured during a patient scan; and
30 a processor in communication with the calibration memory and with the data memory which calculates the calibration parameters by a minimization

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algorithm that includes optimizing fitting parameters with respect to acquired radiation data associated with a point radiation source.

5 15. The imaging system of claim 14 wherein the minimization algorithm further includes:

 calculating lines of response (LOR) based upon the fitting parameters and the measured data;
 generating a figure of merit characterizing the apparent size of the point radiation source based upon the LOR's; and
 10 optimizing the fitting parameters to produce a minimized figure of merit.

15 16. The imaging system of claim 15 wherein the calibration parameters include:

 parameters relating to positional coordinates of the plurality of detectors.

20 17. The imaging system of claim 16, wherein:
 the gantry is a rotatable gantry which acquires measured data over a range of gantry angular positions.

25 18. The imaging system of claim 14, wherein:
 the figure of merit is generated by summing the square of a distance of closest approach of each LOR to a spatial point; and
 the fitting parameters include the positional coordinates of the spatial point.

30 19. The imaging system of claim 14, wherein the generating of the figure of merit includes:
 obtaining a crossing point of each pair of LOR's; and
 calculating a variance of the crossing points.

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20. The imaging system of claim 14, wherein the minimization algorithm further includes:
discarding measured data about radiation events whose energy is outside a preselected energy range.